



**PIONEERS**

INNOVATION FOR RIDER SAFETY



**Improvement of the frontal thorax airbag test procedure for assessing the protection of motorcyclists in a more realistic impact scenario**

# IMPROVEMENT OF THE FRONTAL THORAX AIRBAG TEST PROCEDURE FOR ASSESSING THE PROTECTION OF MOTORCYCLISTS IN A MORE REALISTIC IMPACT SCENARIO

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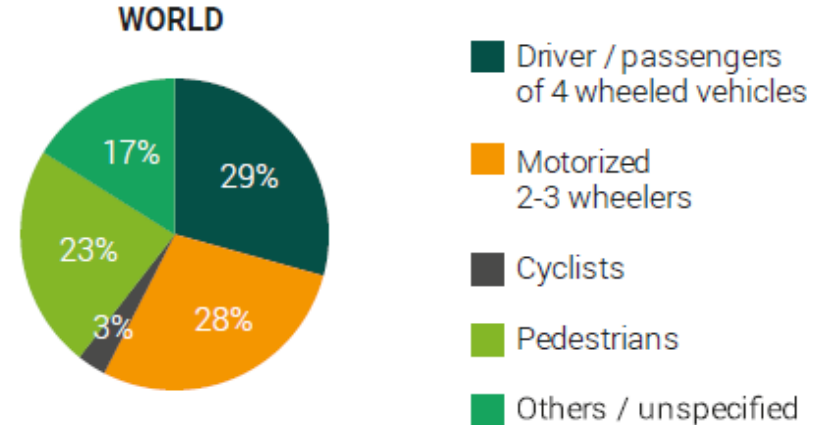
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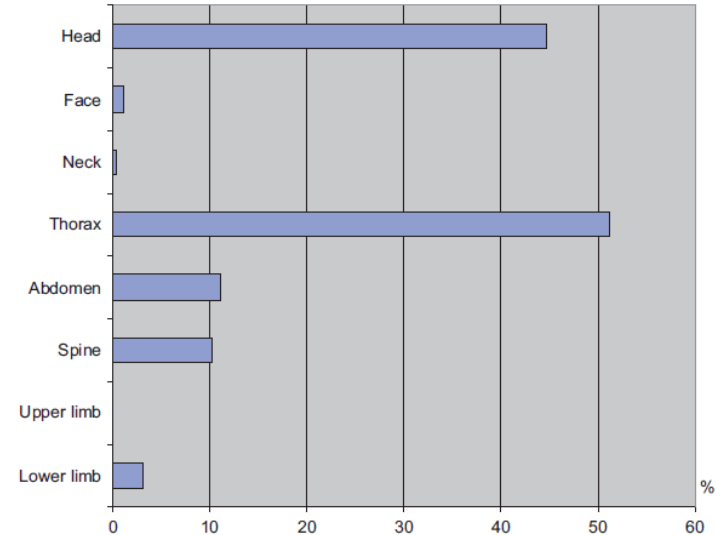
# Introduction

- Powered Two-Wheelers are one of the most dangerous mode of transportation. Higher risk of fatal accident (Bauer et al. 2014)
- Motorcyclists and moped users account 28% of all world traffic accidents. (WHO,2018). 17 % in the European Union (ERSO, 2018).
- Germany: 619 riders dead and 10220 PTW severe injured in 2018 (DESTATIS, 2018).



# Introduction

- Low extremities the most frequently injured. Thorax and head, the most severely body regions injured (MOSAFIN, 2012).
- Thorax is the forth most frequent body region injured but the one with the highest rate of MAIS 3+ injures (more than 50%) (MAIDS, 2008).
- More than 50% of potential fatal injuries (AIS 4+) located in the thorax (Serre et al. 2012).



# Introduction

- Personal Protective Equipment (PPE)
  - Cushion pad: non-inflatable protector
  - Airbag: inflatable protector



[www.dainese.com](http://www.dainese.com)



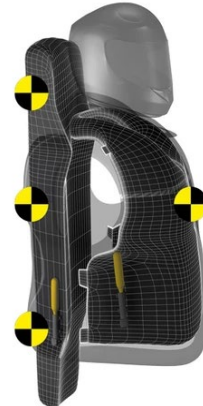
[www.alpinestars.com](http://www.alpinestars.com)



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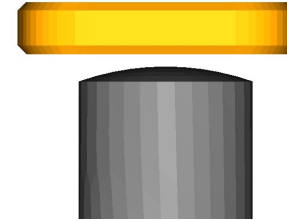
THORAX

[www.motoairbag.de](http://www.motoairbag.de)

# INTRODUCTION

## EN1621-4:2012

- Protection of an inflatable device triggered mechanically.
  - Impact force attenuation.
  - Intervention time: activation time + inflation time.
  - Duration of the inflated status.



5 kg striker  
4.5 m/s  
Steel anvil

$$t_a = d + \frac{l_m - l_i}{s} \times 1000;$$

	<b>Level 1</b>	<b>Level 2</b>
Overall Mean value	≤ 4,5 kN	≤ 2,5 kN
Single strike	≤ 6 kN	≤ 3 kN

# INTRODUCTION

## EN1621-4:2012

- Low biofidelity.
- Low correspondency with realitiy: 50 J impact energy level considerably less than realistic accident impact energy (Ballester et al. 2019, Wei et al. 2020).
- Unknown origin of the impact thresholds.
- Limitations to distinguish the optimal thickness/pressure combination (Aranda et al. 2020).
- Autonomous-triggering devices not considered.





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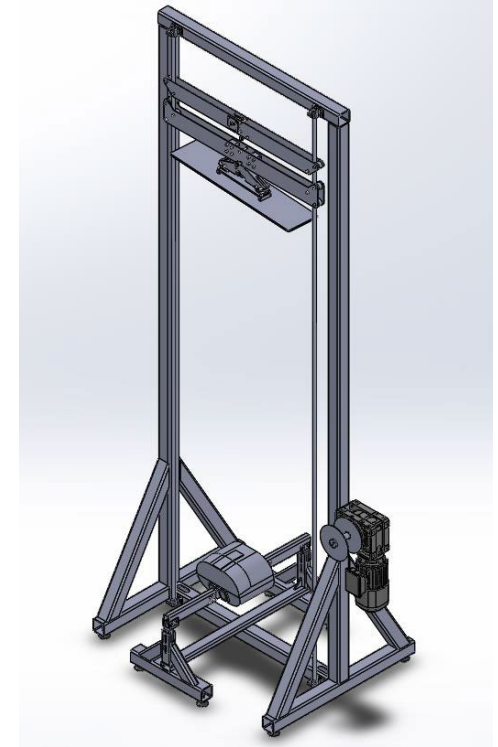
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# TEST METHOD 1

- Robust
- Simple
- Repeatable
- More biofidelic
- More realistic



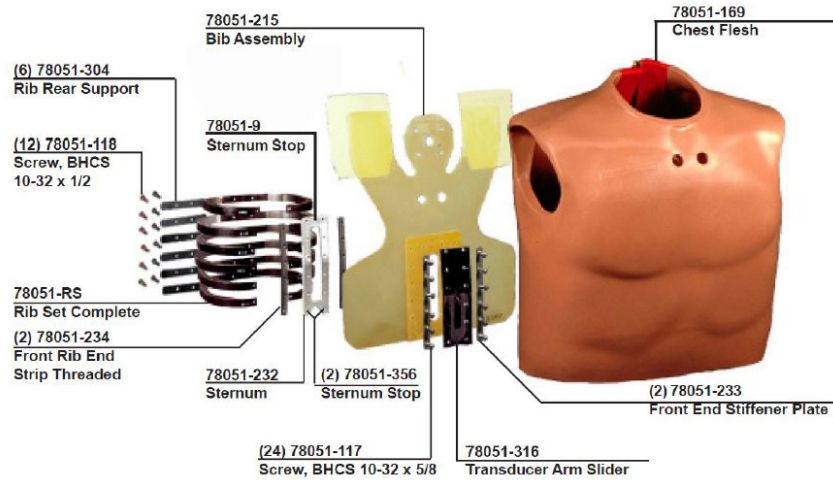
- Drop-Tower
- Guided Free-Fall
- Striker: modular mass
- Human surrogate
- Airbag inflated



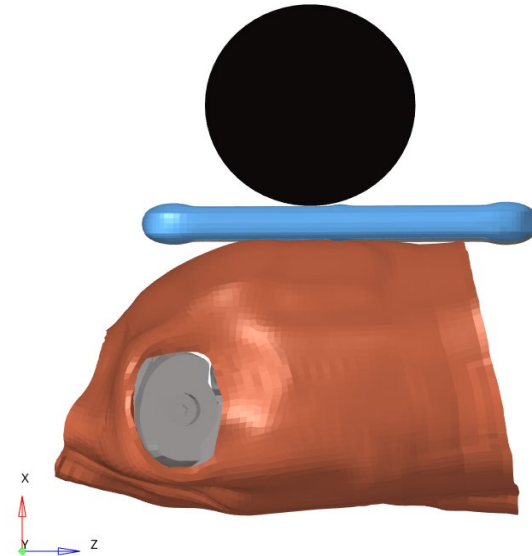
*PIONEERS D3.1*

# TEST METHOD 1

- Human Surrogate: Torso of the 50th percentile Hybrid III Dummy



PIONEERS D3.2



# TEST METHOD 1 – Impact Conditions from Accident Data

## 1) Condition A

Velocity: 3 m/s  
Rigid plane  
Moving mass  $\approx$  75 kg (50th percentile male)



→ Covers 75% cases reported by UGE, in accordance with LMU study

## 2) Condition B

Velocity: 7 m/s  
Rigid cylinder radius 5 to 10 cm.  
Moving mass  $\approx$  75 kg (50th percentile male)



→ Covers 75% of rider to car impacts by UGE.  
→ Major cluster in LMU severe/fatal cases

## 3) Long term update (not now)

Velocity: between 13 and 17 m/s  
Rigid impactor between 5 and 25 cm radius  
Moving mass  $\approx$  75 kg (50th percentile male)

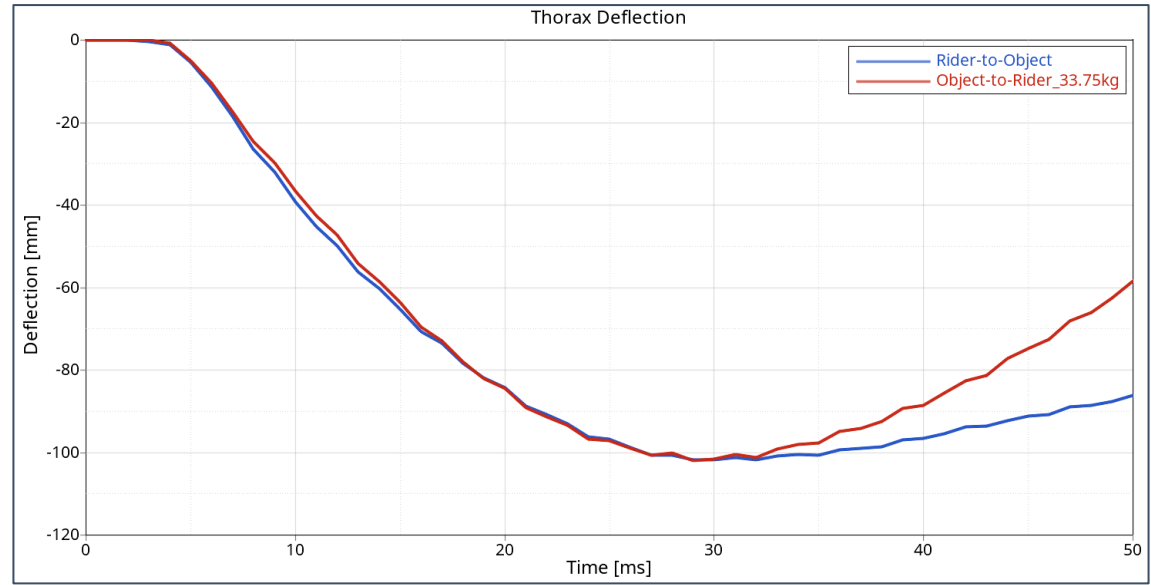
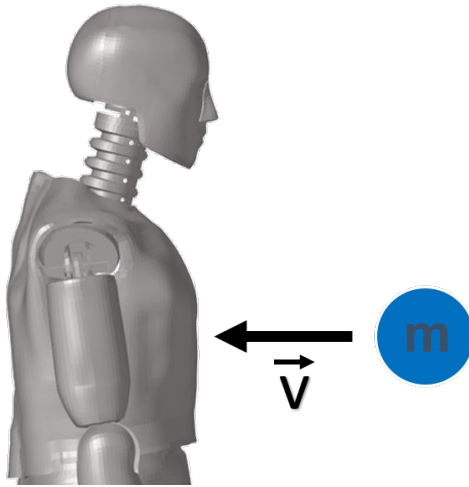


→ Important cluster in LMU severe/fatal cases

# TEST METHOD 1 – Equivalent Mass

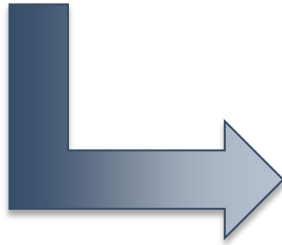
- More realistic

Rider-to-object vs Object-to-rider → mass of the striker?



# TEST METHOD – Test impact conditions: adaptation

- Thorax deflection for equivalent mass at 7 m/s: 102 mm.
- Limit of Hybrid III dummy torso without breaking it: 60 to 70 mm.



Impact conditions	Deflection (mm)
35 kg, 4 m/s	64
35 kg, 3.5 m/s	56,7
10 kg, 7 m/s	56
15 kg, 7 m/s	67,3

# TEST METHOD 1 - Performance

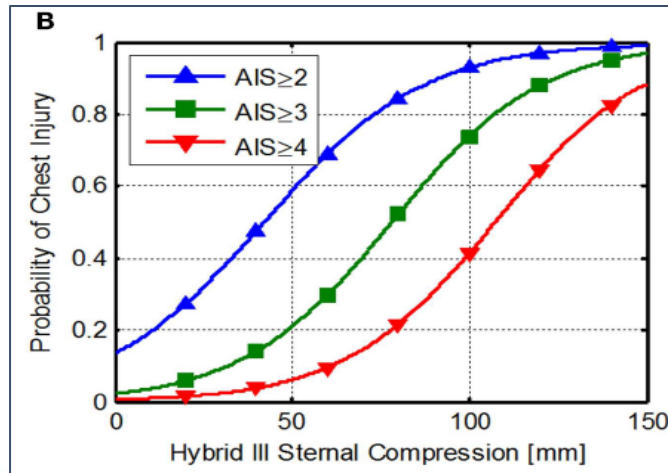
- Protection performance according to biomechanical parameter and criteria.
  - Compression Criteria
    - Based on Kroell et al. 1972, 1974.
    - Thorax deflection.
    - Skeletal Injuries.
  - Viscous Criteria
    - Based on Viano et al. 1988.
    - Viscous response
    - Soft tissue injuries

$$AIS = -3,78 + 19,56C$$

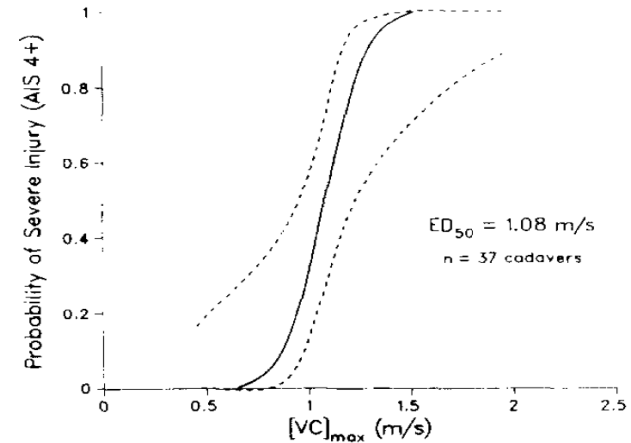
$$VC = V(t) \times C(t) = \frac{d[D(t)]}{dt} \times \frac{D(t)}{b}$$

# TEST METHOD 1 - Performance

- Protection performance based on according to biomechanical parameter and criteria.
  - Compression Criteria



- Viscous Criteria  $VC_{cert} = 1.3 \times VC_{int}$



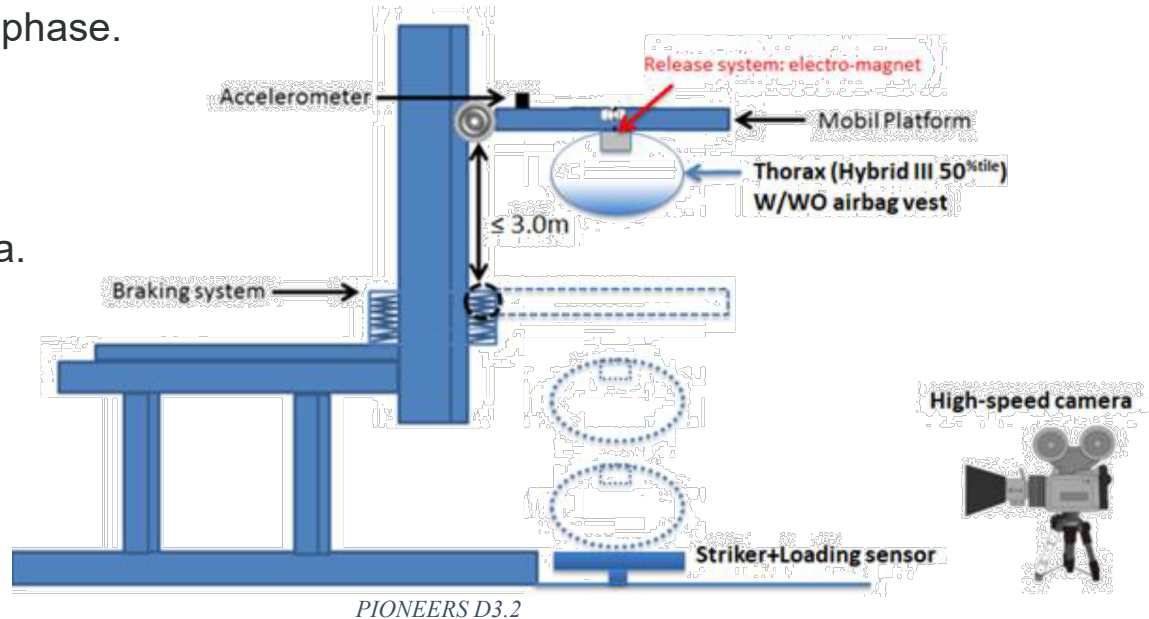


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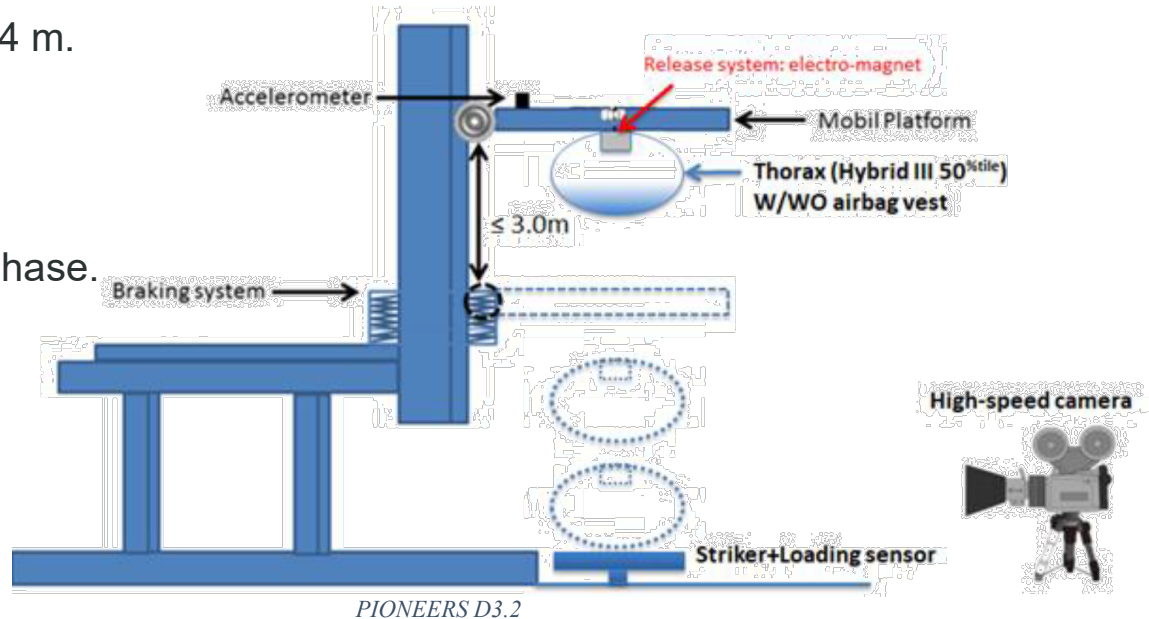
## TEST METHOD 2

- Evaluation of airbag protection performance including inflation phase.
- Mechanical and electrical activation.
- Rider-to-object configuration.
- Based on biomechanical criteria.



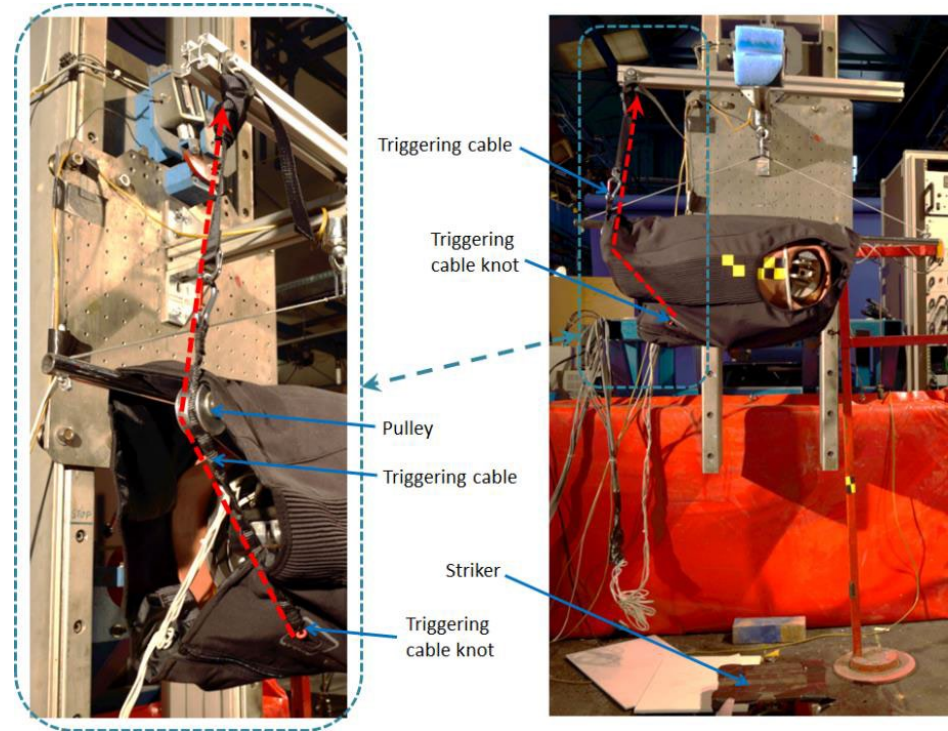
## TEST METHOD 2

- Drop-Tower System.
- Different height positions up to 4 m.
- Hybrid III Dummy torso.
  - Thorax deflection.
  - Viscous response
- High-speed Camera: Inflation phase.
- Flat striker (21.5x27.5x1.5 cm)
- Load cell



## TEST METHOD 2

- More realistic (rider-to-object configuration) but also more complex.
- The mass of Hybrid III dummy torso around 19 kg might not be close to the mass involved in a real accident.



*PIONEERS D3.2*

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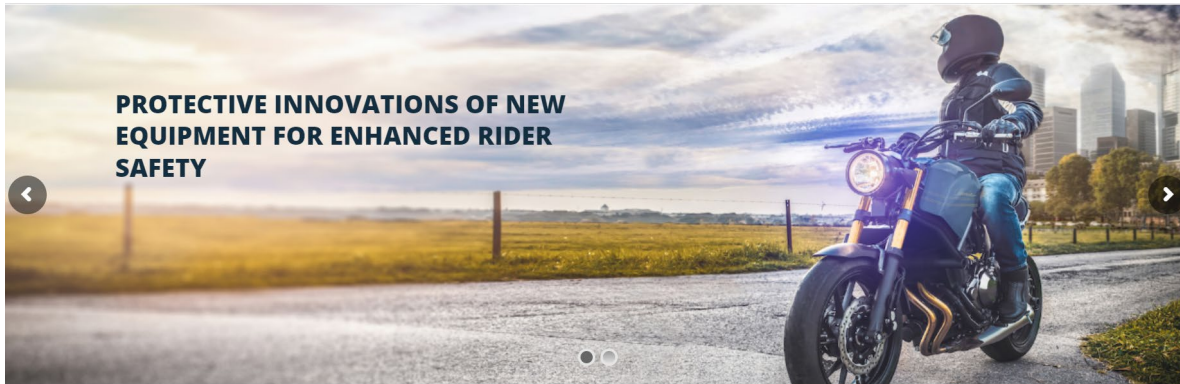
# SUMMARY AND CONCLUSION

- The doubts emerged about the current standard procedure together with its limitations motivated the research of a new test procedure for the performance evaluation of thorax airbags.
- PIONEERS proposed two approaches. Performance evaluation based on biomechanical criteria and parameters.
  - Complement to EN1621-4 to improved evaluation of protection performance in a short/midterm.
  - Procedure to evaluate inflatable devices in a long-term able to combine the evaluation of the protection performance of a real impact scenario with the assessment of the inflation phase.

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**Thank you four your attention**

**Questions?**

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